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Spatiotemporal phase synchronization in adaptive reconfiguration from action observation network to mentalizing network for understanding other's action intention

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Abstract

In action intention understanding, the mirror system is involved in perception-action matching process and the mentalizing system underlies higher-level intention inference. By analyzing the dynamic functional connectivity (DFC) in α (8-12Hz) and β (12-30Hz) frequency bands over a "hand-cup interaction" observation task, this study investigates the topological transition from the action observation network (AON) to the mentalizing network (MZN), and estimates their functional relevance for intention identification from other's different action kinematics.

Sequential brain microstates were extracted based on event-related potentials (ERPs), in which significantly differing neuronal responses were found in N170-P200 related to perceptually matching kinematic profiles and P400-700 involved in goal inference. Inter-electrode weighted phase lag index (WPLI) analysis on the ERP microstates revealed a shift of hub centrality salient in α frequency band, from the AON dominated by left-lateral frontal-premotor-temporal and temporal-parietooccipital synchronizations to the MZN consisting of more bilateral frontal-parietal and temporal-parietal synchronizations.

As compared with usual actions, intention identification of unintelligible actions induces weaker synchronizations in the AON but dramatically increased connectivity in right frontal-temporal-parietal regions of the MZN, indicating a spatiotemporally complementary effect between the functional network configurations involved in mirror and mentalizing processes. Perceptual processing in observing

1 usual/unintelligible actions decreases/increases requirements for intention inference,
2
3 which would induce less/greater functional network reorganization on the way to
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5 mentalization. From the comparison, our study suggests that the adaptive topological
6
7 changes from the AON to the MZN indicate implicit causal association between the
8
9 mirror and mentalizing systems for decoding others' intentionality.
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14 **Keywords:** action intention understanding; ERP brain microstate; dynamic functional
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16 connectivity; action observation network; mentalizing network
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1 Introduction

Understanding others' goals and motives underlying their actions is crucial for communication between individuals who live in the social world. From others' distinct patterns of kinematics, action intentions may be distinguished via direct perception or via inferential processes, which are thought to rely on the mirror system, *i.e.*, action observation network (AON), mapping visual information onto the motor representation in our memory of our own actions, or the mentalizing system enabling us to extract and understand others' goals, thoughts, and beliefs by drawing on "social intelligence" (Becchio et al. 2012; Brass et al. 2007; Catmur 2015; Liew et al. 2011; Rizzolatti et al. 2001; Van Overwalle and Baetens 2009; Woodward and Gerson 2014).

Through low-level perceptual input, the mirror system might result in direct awareness of the goal of a perceived action, by recognizing what is being done and how an action is being performed, especially for familiar or frequently executed actions (Buccino et al. 2004; Decety and Grèzes 1999; Rizzolatti et al. 2007; Van Overwalle and Baetens 2009). At a higher level of understanding why an action is being performed, mirror neurons might respond to acquire actor's immediate intention, on condition that there is contextual information or a specific chain of motor acts (Carter et al. 2011; Catmur 2014, 2015; Ortigue et al. 2009; Woodward and Gerson 2014). While in the absence of contextual information or observing unusual actions, the mentalizing system might be particularly recruited to fill in the "missing"

1 information, by use of the inferential processes to judge others' mental states
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3 (Blakemore and Decety 2001; Becchio et al. 2012; Brass et al. 2007; Catmur 2015;
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5
6 Liew et al. 2011; Van Overwalle and Baetens 2009; Spunt et al. 2011).
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8
9 Brain imaging studies have demonstrated that both mirror neurons and
10
11 mentalizing areas are involved in action intention understanding. Perception of action
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13 kinematics might be an initial stage in the identification of others' intentions, followed
14
15 by the recruitment of inferential processes or other cognitive functions (Becchio et al.
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17 2012; Blakemore and Decety 2001; Catmur 2015; Virji-Babul et al. 2010; Van
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19 Overwalle 2009). However, the transition from mirror to mentalizing system and the
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21 conditions in which each dominates need to be explored (Becchio et al. 2012; Van
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23 Overwalle and Baetens 2009; Tidoni and Candidi 2016). Moreover, functional
24
25 relevance between mirror matching and inferential processes is still unclear and hotly
26
27 debated, especially the role of AON in inferring the goal of an observed action
28
29 (Becchio et al. 2012; Catmur 2015; Marsh et al. 2014; Neal and Kilner 2010; Tidoni
30
31 and Candidi 2016). Some studies argue that the mirror system and the mentalizing
32
33 system are largely mutually independent of each other, because they are rarely
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35 concurrently activated in action intention understanding tasks (Van Overwalle and
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37 Baetens 2009; Virji-Babul et al. 2010). A number of studies suggest that the AON
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39 may support inferential process by providing sensorimotor information to mentalizing
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41 areas for making correct inferences about others' intentions. Nevertheless, more
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43 causal evidence is needed to reveal how these two systems may cooperate and inform
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45 each other (Catmur 2015; Gardner et al. 2015; Tidoni and Candidi 2016).
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1 Recent dynamic network research has provided new insight into dynamic
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3 fluctuations in the brain network structure related to ongoing cognitive function and
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5 the process of replacing one routing function with another while the network keeps
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7 running (Hutchison et al. 2013). Specifically, the topological reorganization of the
8
9 functional brain network has been found to be modulated by cognitive load and
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11 individual's mental effort, *i.e.*, engaged proportion of the total amount of cognitive
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13 resources needed to complete a task (Bassett et al. 2006; Kitzbichler et al. 2011). The
14
15 mentalizing system activation shows the load-dependent increase, in particular, during
16
17 social cognitive information processing (Meyer et al. 2012; Spunt et al. 2013). Thus,
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19 in this study we assume that the perceived visual information in action observation
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21 process imposes different cognitive loads on an observer during higher-level goal
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23 inference, which probably modulates functional integration among brain areas in the
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25 mentalizing network (MZN).
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36 Using a "hand-cup interaction" observation task, dynamic functional connectivity
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38 (DFC), *i.e.*, functional connectivity changing over a short time, was investigated in
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40 this study to estimate the evolving and interconnected nature in the transition from the
41
42 AON to the MZN. To test the interactive relationship between the two functional
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44 networks, the DFC of observing actions performed in an intention-oriented usual way
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46 was compared with that in a non-intentional unintelligible way, since the two types of
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48 actions have different cognitive demands in mirror matching and intention inference
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50 processes. Technically, the timing and localization of mirror responses and
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52 mentalization were determined by event-related potential (ERP) and source trace, and
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1 the DFC of functional brain networks in the time intervals of ERP components was
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3 measured by computing phase synchronization and evaluated according to graph
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5 theory. After that, identifiable spatiotemporal EEG features were identified for
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7 recognizing different types of action intentions. According to the DFC changing over
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9 the task course, the conditions under which the AON is dominated or interrupted by
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11 the MZN, and functional relevance between the topological organizations of AON and
12
13 MZN were analyzed and discussed.
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21 **2 Materials and Methods**

22 **2.1 Participants**

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25 This study recruited 30 college students from Southeast University to participate in
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27 the EEG experiment. Exclusion criteria of subjects included left handedness, medical,
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29 neurological, or psychiatric illness, and history of brain injury or surgery. After
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31 excluding the data seriously contaminated by noise, artifacts or movements, effective
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33 data of 24 subjects composed of 10 males and 14 females aged 22.4 ± 2.3 (mean \pm SD)
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35 were retained and analyzed. The study was approved by the Academic Committee of
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37 the Research Center for Learning Science, Southeast University, China. All the
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39 subjects were asked to read and sign a fully informed consent form for this
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41 experiment and received payment for their participation.
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53 **2.2 Experimental paradigm**

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57 In this experiment, all the participants were asked to view three "hand-cup
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1 interaction" actions performed by a person, which were recorded as stationary frames,
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3 including two typical intention-oriented actions, rather usual in normal life, and a
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5 non-intentional action unintelligible to normal observers. The task was adapted from
6
7 that designed in the study of Ortigue et al. (2009). All the stimuli were presented in
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9 the E-prime 2.0 procedure.
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14 Fig. 1A illustrates the three actions in "no context" condition: 1) Use grip (Ug): a
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16 right hand is grasping a cup for the purpose of using it; 2) Transport grip (Tg): a right
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18 hand is grasping a cup for the purpose of moving it; 3) Simple contact (Sc): a right
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20 hand is touching a cup without a clear purpose.
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25 The experimental task includes a "Ug" condition, a "Tg" condition, and an "Sc"
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27 condition. Each condition consists of 98 trials, resulting in 294 trials in total. In each
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29 task condition, the performer's hand motions were the same across trials, but the cup
30
31 was randomly marked with one of 7 standard colors with equal probability, so each
32
33 color was repeatedly used 14 times. The trials from "Ug", "Tg" and "Sc" conditions
34
35 were cross-presented with a pseudorandom probability. Consecutive presentation of
36
37 the same hand motion was preset as less than 4 times, and the same constrain was set
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39 for the presentation of cups with the same color.
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47 The time for each subject to conduct the experiment was about 24 minutes. The
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49 stimuli were presented sequentially along the timeline illustrated in Fig. 1. The
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51 presentation order and duration are shown in Fig. 1B. After the symbol "+" at the
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53 center of screen presented for 150 ms, a cup was shown for 500 ms. Then a hand
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55 interacted with the cup appeared on the screen for 2000 ms. When the hand-cup
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1 interaction action was presented, subjects were asked to judge the intention of the
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3 actor, which was supposed to be conducted just in their brains without pressing any
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5 button. Before the onset of the next trial, the symbol "+" was shown again with a
6
7 random time length ranging from 1000 ms to 2000 ms as the inter-trial interval.
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10 Before the formal experiment, a practice session including 12 trials was conducted by
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12 each subject, in which each hand motion was repeatedly presented 4 times.
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18 **2.3 EEG recording and preprocessing**

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21 The EEG data were recorded by the Neuroscan international 10-20 system with a
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23 sampling rate of 500 Hz, using 60 electrodes covering frontal, parietal, temporal, and
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25 occipital regions. Additionally, two reference electrodes were placed on the bilateral
26
27 mastoids of subjects, and four surface electrodes simultaneously recording
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29 electrooculographic (EOG) signals were used to monitor ocular movements and eye
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31 blinks, with one pair placed over the higher and lower left eyelids and the other pair
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33 placed 1 cm lateral to the outer corner of the left and right orbits.
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41 The raw EEG data were then preprocessed by the Scan 4.3 software. The
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43 continuous signals were band-pass filtered within a frequency band range of 1-60 Hz.
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45 Each trial was further extracted within a time window of 1200 ms, including 200 ms
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47 for the pre-stimulus period and 1000 ms for the post-stimulus period. The time point
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49 dividing pre- and post- stimuli is the onset of hand-cup interaction action along the
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51 timeline of stimulus presentation (Fig. 1B). The baseline correction was performed
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53 following the pre-stimulus time interval and ocular artifacts were removed according
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1 to the simultaneously recorded EOG signals. After the artifact rejection with
2 thresholds ranging from 50 μv to 75 μv , the trials contaminated by eye blinks and
3 electrocardiogram noise were excluded. Furthermore, the independent component
4 analysis (ICA) plugged in the EEGLAB toolbox was conducted to clear visible
5 artifacts, such as the components of ocular and muscle movements (Delorme and
6 Makeig 2004).
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17 The EEG data across subjects from the three conditions were divided into "Ug",
18 "Tg", and "Sc" groups, consisting of 1146, 1174, 1139 trials respectively, of which
19 36~68 trials were retained under each condition for each subject.
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26 **2.4 ERP brain microstate analysis and source estimation**

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28 To dissociate the cognitive brain states involved in the action intention understanding
29 task, we used ERPs and difference waveforms to establish the time course during
30 which the processes of mirror matching and intention inference occur instantaneously.
31 The ERPs were found being elicited in different action intention discrimination tasks,
32 within which neural responses to the observed actions significantly differ as an
33 indicator of visual perception and goal inference (Ortigue et al. 2009, 2010; Van
34 Overwalle et al. 2009; Van der Cruyssen et al. 2009; Vistoli et al. 2015).
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49 ***Sequential ERP microstates:*** Firstly, a micro-segmentation of standard ERP
50 components was conducted to construct sequential stable microstates with
51 representative configuration of global electric potential (Cacioppo et al. 2014; Khanna
52 et al. 2015). A microstate refers to momentary, patterned, and quasi-stable global
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1 functional state of the brain, and reflects a time-limited information processing
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3 operation (Koenig et al. 2002). Event-related brain microstates can reflect different
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5 cognitive functions, such as perception, attention, disease, emotion, and reasoning
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7 (Milz et al. 2016). For the data from each task condition, an averaged ERP file across
8
9 all the trials and subjects was created. The ERP waveform can be represented as a
10
11 $T \times n$ matrix with T being the number of timeframes and n the number of EEG
12
13 channels. The averaged ERP data were processed by using the Chicago
14
15 Electro-Neuroimaging Analytics (CENA) toolbox (Cacioppo et al. 2014; Cacioppo
16
17 and Cacioppo 2015). Unlike the traditional methods for extracting microstate
18
19 topology, such as k -means clustering method, the CENA performs a data-driven
20
21 (automatic) detection of non-periodic quasi-stable brain states through parsing the
22
23 ERPs into the baseline state, stable microstates, and non-stable transitions between
24
25 these states. The micro-segmentation by the CENA tool was conducted in four major
26
27 steps: 1) Root mean square error (RMSE) metric was computed for identifying the
28
29 transitions across discrete microstates; 2) Global field power (GFP) was estimated to
30
31 discover the changes in the overall level of brain activation; 3) Based on cosine
32
33 distance between the template maps derived from the 60-dimensional sensor space for
34
35 successive evoked microstates, similarity metric was computed to confirm whether
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37 the microstates identified in terms of the RMSE differ in the configuration of brain
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39 activity; 4) Bootstrapping procedure was performed for identifying heterogeneities in
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41 the timing or number of microstates as well as their representative template maps
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43 across subjects.
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1 ***Difference wave analysis:*** Secondly, a "difference waveform" between ERPs was
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3 computed to isolate the components of interest, since difference wave was thought to
4
5 represent psychological processes that are different between two conditions. In this
6
7 study, difference wave configuration was created between 60-dimensional ERPs by
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9 subtracting the ERP waveform elicited by one condition from the ERP waveform
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11 elicited by another, and topological maps of difference waveforms with GFP peaks
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13 were constructed for every pair of task conditions to test within-subject effect on brain
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15 states.
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21 ***Cortical source estimation:*** Finally, the cortical source of every stable microstate
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23 was estimated by using a cortical source estimation procedure implemented in the
24
25 Brainstorm toolbox (<http://neuroimage.usc.edu/brainstorm>; Tadel et al. 2011), and the
26
27 source current of difference waveform was estimated as well. The EEG signals were
28
29 assumed to be generated from a block of electric dipoles at the cortical surface. The
30
31 forward model was calculated with a symmetric Boundary Element Model (BEM) in
32
33 OpenMEEG, an open-source software ([http://www-sop.inria.fr/athena/software/](http://www-sop.inria.fr/athena/software/OpenMEEG/)
34
35 OpenMEEG/; Gramfort et al. 2010), on the cortical surface of a template MNI brain
36
37 ("Colin27" atlas), with a 1 mm resolution. Specifically, the noise of the scalp sensors
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39 was removed through computing the noise covariance matrix of the signals in the
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41 pre-stimulus time interval. Cortical sources were estimated by means of an inverse
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43 kernel matrix that had been produced by the forward model and the standardized Low
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45 Resolution Brain Electromagnetic Tomography (sLORETA) estimation algorithm.
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1 of 15,002 elementary current dipoles.
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4 **2.5 WPLI analysis and construction of functional microstate networks** 5 6 7

8 To investigate how action perception and intention inference modulate local
9 specialization and inter-regional integration in the brain, functional networks of
10 event-related oscillations were constructed in the temporal windows of ERPs. It has
11 been suggested that true interaction between two neural sources results in a coherent
12 phase relationship between their corresponding time series, which is represented by a
13 value ranging from 0 and π (Vinck et al. 2011).
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24 *Inter-trial coherence of principle components:* The assessment of functional
25 connectivity is based on an analysis of phase synchrony between pairwise EEG
26 signals in α (8-12Hz) and β (12-20Hz) frequency bands. The frequency selection was
27 determined by an inter-trial coherence (ITC) analysis for the principle components
28 located at left and right cerebral hemispheres, because ITC can statistically detect the
29 time-frequency regions with event-related phase-locking events for all trials in a
30 dataset (Delorme and Makeig 2004) (Fig. 2).
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44 *Association matrix of phase synchronization:* Centering around the time point of
45 the GFP peak of each ERP component, consecutive functional microstate networks
46 were constructed with the 60 EEG channels used as the nodes. The length of each
47 time window of a microstate network is at least 100 ms, to ensure that at least one
48 cycle is available for estimating phase relationship between neural signals in α and β
49 frequency bands. It is well-known that volume conduction can cause spurious increase
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1 of connectivity between sensors. In order to reduce sensitivity to additional and
 2 uncorrelated noise sources and increase statistical power in detecting true changes in
 3 phase synchronization, weighted phase lag index (WPLI) (Vinck et al. 2011) was used
 4 to measure the existence of time-lagged interdependence between two time series of
 5 EEG signals.
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14 The basic idea of phase lag index (PLI) is to investigate the asymmetry of the
 15 distribution of phase differences around zero, which is given by
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$$19 \quad PLI = |\langle sign(\Delta\phi_{rel}(t)) \rangle| = \left| \frac{1}{X} \sum_{x=1}^X sign(\Delta\phi_{rel}(t_x)) \right|$$

20 where $\Delta\phi_{rel}$ is phase difference at time-point x between two time series, which is
 21 determined for all time-points ($x = 1 \dots X$) per time window, *sign* stands for signum
 22 function, $\langle \rangle$ denotes the operation of mean value, and $||$ indicates the absolute value.
 23
 24 Instantaneous phases were determined by the Hilbert transformation, applying a
 25 Hanning window on the concurrent fast Fourier transform. The range of the PLI value
 26 is $[0,1]$, with 0 denoting no coupling or coupling with a phase difference centered
 27 around $0 \bmod \pi$ and 1 representing perfect phase locking at the values of $\Delta\phi_{rel}(t)$
 28 different from $0 \bmod \pi$. Although PLI shows robustness against the presence of
 29 common sources, *i.e.*, volume conduction and the possibly active reference in EEG, it
 30 is biased and loses some ability to detect changes in phase synchronization of noisy
 31 signals, especially in the case of weak coupling (Vinck et al. 2011).
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54 As a weighted version of PLI, WPLI has been recently developed to tackle the
 55 problems of small-magnitude synchronization effect existing in PLI. WPLI weights
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1 each phase difference according to the magnitude of the imaginary component of the
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3 cross-spectrum, therefore, phase differences around zero only marginally contribute to
4
5 the calculation of WPLI. Since the contribution of the observed phase leads and lags
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7 is weighted, WPLI presents "reduced sensitivity to uncorrelated noise sources and
8
9 increased statistical power to detect changes in phase synchronization (PS)" (Vinck et
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11 al. 2011).
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17 Through computing WPLI for each pair of EEG time series averaged across trials
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19 for each task condition and for each subject, sequential 60×60 association matrices
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21 were created for the brain microstates changed over the task course.
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25 ***Undirected network construction:*** For each association matrix, an adjacent
26
27 matrix was acquired through applying a threshold by the following steps: 1) In the
28
29 pre-stimulus period, a fixed connection density p was set abiding by the Erdős-Rényi
30
31 model (1961) for each subject (*i.e.*, $p = 2\ln n/n$, where n is the number of the
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33 nodes, *i.e.*, channels), to get a no-task WPLI adjacency matrix; 2) the minimum
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35 WPLIs of all the pre-stimulus adjacency matrices from the 24 subjects were averaged;
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2.6 Functional connectivity and network topology metrics of sequential graphs

To assess the DFC of the brain network, the global structure and local node

1 characteristic of the sequential graphs were measured according to graph theory
 2
 3 (Bullmore and Sporns 2009; Rubinov and Sporns 2010). Global integration of a
 4
 5 functional network was estimated by using connection density and characteristic path
 6
 7 length. While assessing local specialization of a functional brain network, we focused
 8
 9 on a particular type of graph-based method that identifies the nodes that play central
 10
 11 roles within the network structure. Specifically, centrality measures make implicit
 12
 13 assumptions about the manner in which traffic flows through a network (Lohmann et
 14
 15 al. 2010; Opsahl et al. 2010; Sporns et al. 2007). According to the suggestion of
 16
 17 Sporns *et al.* (2007), a combination of various graph measures, named "node
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 19 centrality", was employed here to characterize such nodes, including degree,
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 21 betweenness and closeness centrality.
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31 According to the definitions from graph theory, N is the set of all the nodes in a
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 33 network and (i, j) represents the edge between nodes i and j ($i, j \in N; i \neq j$). If
 34
 35 there is connection status between nodes i and j , $a_{ij} = 1$; otherwise, $a_{ij} = 0$. The
 36
 37 following graph metrics can be estimated based on the connectivity matrix defined by
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 39 a_{ij} .
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45 **Connection density:** It refers to the number of edges in a graph comprising n
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 47 nodes divided by the maximum number of possible edges $[(n^2 - n)/2]$.
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50 **Characteristic path length:** It is the average number of edges in the shortest paths
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 52 between all the nodes, *i.e.*,
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$$L = \frac{1}{n} \sum_{i \in N} L_i = \frac{1}{n} \sum_{i \in N} \frac{\sum_{j \in N, j \neq i} d_{ij}}{n - 1}$$

1 where L_i is the average distance between node i and other nodes, and $d_{ij} =$
2
3 $\sum_{a_{uv} \in g_{i \rightarrow j}} a_{uv}$ refers to the shortest path length between nodes i and j ($g_{i \rightarrow j}$ is the
4
5 shortest geodesic path between i and j). For all the disconnected node pairs i and j ,
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9 $d_{ij} = \infty$.

10
11 **Node connection strength:** It refers to the sum of weights attached to ties
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13 belonging to a node in a weighted network. In this study, connection strength of node
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17 i is given by the sum of the WPLIs of the adjacent edges connected to the node.

$$20 \quad s_i = \sum_{j \in N} a_{ij} w_{ij}$$

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24 where w_{ij} is the WPLI between node i and node j .

25
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27 In the following computations for the three measurements of node centrality, edge
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29 weights were added to the graph that roughly correspond to the length of the paths,
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32 which had been calculated using the Euclidean distance between the coordinates of
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35 the end nodes of each edge.

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38 **Degree centrality:** Node degree is the most fundamental network measure, which
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41 is quantified by the number of connections linked to node i :

$$43 \quad k_i = \sum_{j \in N} a_{ij}$$

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47 A node with high degree centrality is viewed as a "pivotal hub" in a network.

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50 **Closeness centrality:** The closeness centrality of node i is calculated as the
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52
53 inverse of the average distance from this node to all other nodes in the network (*i.e.*,
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55
56 the inverse of the row mean of the distance matrix):

$$C_i = \frac{n-1}{\sum_{j \in N} d_{ij}}$$

Closeness centrality measures how many steps, on average, a node takes to reach everyone else in the network. Thus, the distance from a node with high closeness centrality to any other node is short on average. These nodes are considered to be structurally important, because they can easily reach or be reached by others.

Betweenness centrality: It is measured based on the proportion of the number of the shortest paths between all node pairs, which pass through a specific node, to the total number of shortest paths between all node pairs. The measurement can assess the communication role of the node within the functional network. It is defined as follows:

$$b_i = \frac{1}{(n-1)(n-2)} \sum_{\substack{h, j \in N \\ h \neq j, h \neq i, j \neq i}} \frac{\rho_{hj}(i)}{\rho_{hj}}$$

where ρ_{hj} is the number of the shortest paths between nodes h and j , and $\rho_{hj}(i)$ is the number of the shortest paths between nodes h and j that pass through node i . Nodes with high betweenness centrality are crucial to play the role of "connector hub" in a network.

2.7 Statistical and discriminate analyses of differences between action intentions

Using the 24 subjects as the testing samples, the amplitudes of ERPs from 60 channels elicited by different task conditions were statistically tested by the paired Student's t-tests. Additionally, to detect the systematic differences in functional connectivity of α - and β -band phase-synchronized networks, the graph-theoretical

1 measurements of global topology and local nodes between every two conditions were
2
3 statistically compared by the paired Student's t-tests. A false discovery rate (FDR)
4
5 procedure was used to correct for multiple hypothesis testing, with significance level
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7 set to 0.05. The null hypothesis is that there is no difference between task conditions.
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9

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11 For α - and β -band functional networks, connection strengths of each EEG
12
13 electrode were extracted in the temporal windows of N170-P200 and P400-700
14
15 responses to constitute two-dimensional input features for the discriminant analysis
16
17 between task conditions. Then the subject-based feature samples were recognized
18
19 using linear discriminant analysis (LDA), support vector machine (SVM) and Naive
20
21 Bayes individually, to find the distinguishable electrode sites from the time-varying
22
23 functional connectivity microstates in identifying other's different action intentions.
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31 **3 Results**

32 **3.1 Time-locked ERP brain microstates and source localization**

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39 The grand average of ERPs from EEG midline electrodes in "Ug", "Tg", and "Sc"
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41 conditions are shown in Fig. 3. It can be found that N70, P120, N170-P200, P300 and
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43 P400-700 are elicited by the three conditions. Specifically, the disassociations among
44
45 the three ongoing waveforms can be found in representative electrodes FZ, CZ, PZ
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47 and POZ.
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53 Corresponding to the ERPs, continuous brain microstates were constructed for
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55 each task condition by parsing the series of electric potential configurations. Fig. 4
56
57 illustrates the temporal evolution of microstate topologies, in which five stable
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1 microstates under "Ug" condition were retrieved by the CENA procedure after
2
3 excluding transition states with too short duration. Each topological map and source
4
5 distribution correspond to the global potential peak of a representative ERP
6
7 component. For "Tg" and "Sc" conditions, topological maps and source distributions
8
9 can be constructed similarly. The durations and cortical sources of the five
10
11 event-related microstates are summarized in Table 1.
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17 Statistical analysis has revealed the EEG electrode distribution with significant
18
19 disassociations in the ERPs of microstates 2~5, in which the N170-P200 microstate
20
21 has been particularly found having the maximum number of electrodes with
22
23 significant potential difference between "Ug" and "Sc" and between "Ug" and "Tg"
24
25 conditions (paired Student's t-tests with FDR correction: $p < 0.05$) (Fig. 5C and 5E).
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28 The difference waves of N170-P200 are consistently located in left cerebral
29
30 hemisphere, involving the premotor cortex, inferior frontal gyrus (IFG), anterior
31
32 intraparietal sulcus (IPS), superior temporal sulcus (STS) and posterior
33
34 parietooccipital cortices. However, there are no significant potential differences in
35
36 N170-P200 waves in the EEG electrodes between "Tg" and "Sc" conditions (paired
37
38 Student's t-test with FDR correction, $p > 0.05$) (Fig. 5D). On the other hand, the
39
40 P400-700 microstate also shows high sensitivity to different action intentions. The
41
42 brain mapping and source analysis for GFP peaks reveal that the maximum currents in
43
44 P400-700 are distributed at the medial prefrontal cortex (mPFC), anterior cingulate
45
46 cortex (ACC), and right temporo-parietal junction (TPJ) (Fig. 4 and Fig. 5B). As
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48 shown in Fig. 3, there is remarkable differentiation in P400-700 waves among the
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1 three conditions, in which "Sc" condition particularly evokes the highest response
2 amplitude. While compared with "Ug" and "Tg" conditions, difference waves from
3 "Sc" condition are manifested as higher local field potential activities in the mPFC,
4 right IFG, STS, and anterior temporal lobe but less responses in left temporal lobe and
5 posterior parietal-occipital areas (paired Student's t-test with FDR correction, $p < 0.05$)
6 (Fig. 5C and 5D).
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18 **3.2 Event-related phase-synchronized networks over task course**

19 Under the three action intention conditions, the phase-synchronized networks
20 constructed based on the continuous time-locked ERPs are presented in Fig. 6. It can
21 be seen that understanding usual and unintelligible actions generates different levels
22 of event-related functional connectivity and topological reorganization.
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33 Especially at the time intervals with N170-P200 evoked, *i.e.*, the duration of
34 microstate 3, functional connections in α - and β -band networks focus on the frontal,
35 premotor, temporal, parietal and occipital areas in left-lateral cerebral hemisphere.
36 Specifically, there are dense inter-regional phase synchronizations for understanding
37 usual actions in "Ug" and "Tg" conditions. As a contrast, the functional network of
38 N170-P200 shaped under "Sc" condition shows the most sparse connections in both α
39 and β frequency bands, reflecting suppressed synchronized activities for inter-regional
40 information transmission (Fig. 6A and 6B). While in the later phase with P400-700
41 evoked, *i.e.*, the duration of microstate 5, the networks are mainly composed of
42 functional connections distributed in left-lateral frontal-temporal and bilateral
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1 parietal-occipital areas. Right frontal and temporal areas are differentially involved in
2
3 the three task conditions. Especially in "Sc" condition, there are strongly increased
4
5 synchronized activities among prefrontal, inferior frontal, parietal and temporal areas
6
7 in right cerebral hemisphere, which is more salient in the α -band functional network
8
9 (Fig. 6A).
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15 **3.3 Effect of tasks on spatiotemporal evolution of functional connectivity**

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19 The graph-theoretical analysis reveals the temporal evolution of global topology of
20
21 functional brain networks. As shown in Fig. 7A and 7B, following the ERP-indexed
22
23 cognitive microstates, global connection density of α - and β -band event-related
24
25 networks tends to increase gradually, while characteristic path length shows a
26
27 tendency of decrease. The timeline of global network measurements implies that the
28
29 cognitive processing in the later phases (microstates 4~5) recruits more connections
30
31 and so induces strongly enhanced global integration in the networks, which subserves
32
33 strengthened functional connectivity and global efficiency of information
34
35 transmission. While compared with "Ug" and "Tg" conditions, the functional network
36
37 topology in "Sc" condition shows the lowest global connection density and the highest
38
39 characteristic path length in the early phase (statistical significance is partly found in
40
41 paired Student's t-tests on α - and β -band networks: $p < 0.05$; Fig. 7A and 7B), but it is
42
43 organized in an almost reversed way in the later phase, *i.e.*, the highest connection
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45 density and the lowest path length (statistical significance is partly found in paired
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47 Student's t-tests on α -band networks: $p < 0.05$; Fig. 7A), which denotes the greatest
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1 adaptive reconfiguration of functional brain networks in the transition from the earlier
2
3 to the later cognitive sub-processes in understanding other's unintelligible action
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5 intention. Besides, there are no significant differences in global topological
6
7 measurements between the networks shaped in "Ug" and "Tg" conditions.
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11 The analysis of local nodes has revealed a shift of hub centrality following the
12
13 topological reorganization of the event-related networks. Especially in the α -band
14
15 networks derived from N70, P120 and N170-P200 components, it can be found that
16
17 the pivotal hubs with relatively high "degree" centrality scores focus on left central,
18
19 temporal, parietal and occipital areas. However, in the α -band networks corresponding
20
21 to P300 and P400-700 responses, the most pivotal hubs are distributed in right-lateral
22
23 posterior brain areas and inferior frontal lobe. Some nodes in right prefrontal cortex
24
25 (PFC) are particularly involved in "Sc" condition (Fig. 8A). Apart from the changes of
26
27 node degree distribution, α -band networks show local reorganization in the nodes
28
29 with relatively high closeness and betweenness centrality scores, manifested as the
30
31 transition from the left posterior regions in the early event-related networks
32
33 (microstates 1~3) to the right-lateral parietooccipital regions in the networks recruited
34
35 in the later phases (microstates 4~5). The shift of node centrality in the functional
36
37 brain networks denotes the switched role of local neural circuits in the coordination of
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39 information flows of different cognitive sub-processes.
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53 By using the Louvain method for community detection from large-scale networks
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55 (Blondel et al. 2008), all the nodes in the synchronization networks formed in the
56
57 temporal windows of N170-P200 and P400-700 are parsed into the communities with
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59

1 structurally optimized modularity. Based on the Kamada-Kawai method (Kamada and
2
3 Kawai 1989), the major community divisions of each event-related network are
4
5
6 observed in the force-directed connection graph with an optimized node layout (Fig.
7
8
9 9).

10
11 In the temporal networks produced from the three conditions, there are different
12
13 division patterns and sub-components within the communities. In the early period of
14
15 the task, the α -band synchronization networks corresponding to N170-P200 under
16
17 "Ug" and "Tg" conditions can be divided into frontal, premotor-temporal and
18
19 frontal-parietal-occipital communities in left hemisphere (Fig. 9A), and the β -band
20
21 networks mainly contain frontal-temporal-parietal and left-lateral temporal-parietal
22
23 and parietal-occipital communities (Fig. 9B). However, in this period the α -band
24
25 network organized in "Sc" condition is constituted by left frontal-parietal-occipital
26
27 and premotor-temporal-parietal communities, with rather sparse inter-node
28
29 connections and less interconnectivity (Fig. 9A), while the β -band synchronization
30
31 network can be partitioned into frontal and parietal-occipital and left temporal-parietal
32
33 communities (Fig. 9B).
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37 In the later period of the task, *i.e.*, the temporal window of P400-700, it can be
38
39 found that α -band synchronized activities in bilateral frontal-parietal and left
40
41 frontal-temporal-parietal communities dominate the dynamic networking process of
42
43 discrete brain areas. Specifically, there are additional functional divisions in α -band
44
45 networks formed under "Sc" condition, involving left frontal, right frontal-temporal,
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47 and right temporal-parietal communities (Fig. 9A). In addition, β -band
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1 synchronization networks in "Ug" and "Tg" conditions can be divided into
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3 frontal-parietal, frontal-temporal and left temporal-parietal communities, while that in
4
5 "Sc" condition particularly contains a frontal-temporal community at right cortical
6
7 hemisphere (Fig. 9B).
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10 11 12 **3.4 Identifiable EEG channels with time-dependent WPLI differences** 13 14

15
16 In the periods of N170-P200 and P400-700 responses, the WPLI differences between
17
18 task conditions show time-dependent changes with the adaptive network
19
20 reorganization (Fig. 10). While compared with α -band WPLIs formed in "Sc"
21
22 condition, higher synchronizations during the period of N170-P200 are distributed
23
24 among left temporal, parietal and occipital nodes in the networks under "Ug" and "Tg"
25
26 conditions. Conversely, in the later neural response process, "Sc" condition elicits
27
28 higher α -band synchronized activities in right frontal-parietal, frontal-temporal,
29
30 temporal-parietal and parietal-occipital regions, but evokes fewer activities in left IFG,
31
32 as compared to "Ug" and "Tg" conditions (Fig. 10A). In β -band functional
33
34 connectivity microstates (Fig. 10B), there are slightly higher WPLIs in "Ug" and "Tg"
35
36 conditions than those in "Sc" condition during the N170-P200 period. By contrast,
37
38 "Sc" condition elicits relatively increased synchronizations in the temporal window of
39
40 P400-700 than the other two conditions. On the other hand, the comparison performed
41
42 between the two usual actions reveals that, while subtracting synchronized activities
43
44 under "Ug" condition, "Tg" condition only evokes more synchronizations in bilateral
45
46 premotor-parietal areas in N170-P200 period. However, the differences in connection
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1 strengths of individual nodes between "Ug" and "Tg" events are not significant in
2
3 terms of the paired Student's t-tests ($p>0.05$), regardless of the functional connectivity
4
5 microstates in the earlier (N170-P200) or the later (P400-700) period of the task (Fig.
6
7
8
9 10A and 10B).

10
11 Following the topological transformation of the event-related functional
12
13 connectivity microstates, EEG electrodes T7, P2 and FP2 with the connection
14
15 strengths changed from N170-P200 to P400-700 time windows are the distinguishable
16
17 network nodes in recognizing usual and unintelligible action intentions (Fig. 11).
18
19 Within the α -band functional networks, T7 at left temporal lobe, P2 at right superior
20
21 parietal lobe and FP2 on right PFC are found having relatively high accuracies
22
23 (0.6~0.8) in the classifications of "Ug vs. Sc" and "Tg vs. Sc" task conditions,
24
25 whereas there are lower accuracies (<0.6) of the individual nodes within the β -band
26
27 phase-synchronized networks in recognizing the distinctions between task conditions.
28
29 The identifiability of individual nodes at the left temporal and right superior parietal
30
31 brain regions is attributed to the differences between task conditions in the α -band
32
33 temporal-parietal connectivity involved in the earlier N170-P200 period. The right
34
35 prefrontal node distinguishable in understanding different types of action intentions is
36
37 related with the α -band frontal-temporal and frontal-parietal connectivity varying in
38
39 the later cognitive process of P400-700 response (Fig. 10A).
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54 **4. Conclusion and Discussion**

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57 Based on the ERP brain microstates, phase-synchronized networks organized for
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1 different information processing stages of action intention understanding have been
2
3 constructed, in which complex functional interactions among brain areas are mutually
4
5 modulated by different cognitive sub-processes and the type of action intention.
6
7 Moreover, the comparative analysis of DFC has discovered different adaptive
8
9 reorganization patterns of functional brain networks in the intention identification of
10
11 distinct action kinematics, manifested as enhanced/suppressed topological
12
13 configuration of the early event-related network formed in N170-P200 period but the
14
15 subsequent less/greater reorganization toward the functional network in P400-700
16
17 response while understanding usual/unintelligible actions.
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25 ***N170-P200 and P400-700 responses to action perception and intention***
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27
28 ***inference:*** By using the CENA method, this study extracts five consecutive brain
29
30 microstates comprising the ERP components over the task course. Combining the
31
32 psychological processing mechanism with difference waveforms and source
33
34 localization, the N170-P200 microstate is most likely indicative of the mirror
35
36 matching process that acquires information from the actor's action kinematics, and the
37
38 P400-700 microstate conveys information related to higher-level mentalizing process,
39
40 at least to the onset of mentalization, which infers the goals/intentions from the actor's
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42 hand movement.
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50 At the early stage, the initial small negative N70 in microstate 1 is an early
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52 component of visual evoked potential (VEP), primarily located at the occipital cortex.
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54 The time interval has been suggested as the onset of discriminative information of
55
56 action intentions (Ortigue et al. 2009). Since there are no significant differences
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1 among the perceived action kinematics, the N70 microstate might be uncorrelated
2
3 with physical properties of visual input. Microstate 2 (P120) and microstate 3
4
5 (N170-P200) have been found to be generated by the same brain sources, and
6
7 suggested as the sequential neural activities involved in perception of visual materials
8
9
10 (Ortigue et al. 2009; Yang et al. 2011). Especially in the microstate 3, the
11
12 occipitotemporal N170 is a non-specific, motion-related component originating from
13
14 quinary visual cortex/middle temporal area (V5/MT) while P200 around the
15
16 parietooccipital region is known to be sensitive to physical properties of visual stimuli
17
18 (Yamasaki et al. 2012). The cortical source currents corresponding to N170-P200 are
19
20 mostly distributed in the premotor cortex, anterior IPS, and STS in left cerebral
21
22 hemisphere (Fig. 4), which have been recognized as the important brain areas
23
24 critically involved in the mirror system to decode immediate goals of actions (Becchio
25
26 et al. 2012; Van Overwalle and Baetens 2009). More importantly, the time point
27
28 where the waveforms for different kinematics start to differ is the timing of the
29
30 N170-P200 microstate (Fig. 3), indicative of higher sensitivity for physical properties
31
32 of visual stimuli in the action observation-execution matching process. Specifically,
33
34 significant potential differences in N170-P200 between task conditions are
35
36 consistently located in left-lateral brain areas, mainly including the premotor cortex
37
38 and the STS underlying mirror neuron properties and posterior parietooccipital
39
40 regions associated with visual processing (Fig. 5C-5E).
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55 At the later stage, the elicited P300 (P3a) in the microstate 4 covering
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57 frontal-parietal-temporal cortices is believed to reflect attention allocation and
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1 memory updating related to cognitive tasks. The late positive going waveform
2
3 P400-700 (P3b) in the microstate 5 shows striking event-related activations in the
4
5 mPFC, ACC and right TPJ (Fig. 4), which have been suggested as the core regions to
6
7
8 constitute the mentalizing system (Becchio et al. 2012; Brass et al. 2007; Liew et al.
9
10
11
12 2011; Van Overwalle and Baetens 2009). Moreover, remarkable disassociation in P3b
13
14 amplitudes is found among "Ug", "Tg" and "Sc" conditions (Fig. 3). The sources of
15
16
17 difference waves between task conditions focus on right-lateral anterior cortical areas
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19
20 to a great extent, primarily including right IFG, STS and anterior temporal lobe and
21
22
23 the mPFC (Fig. 5C-5E), some parts of which are thought to be devoted to mentalizing
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25
26 process (Carrington and Bailey 2009). Previous studies have generally suggested that
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28
29 P3b reflects central cognitive processes occurring with the active detection of an
30
31
32 attended stimulus and appears related to subsequent memory processing (Polich 2007).
33
34
35 Specifically, P3b amplitude depends on the demands for cognitive capacity.
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38 Subjectively improbable events will elicit a P3b, and the less probable the event, the
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40
41 larger the P3b amplitude (Donchin 1981; Polich 2007). In line with this conclusion,
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43
44 the highest P3b amplitude has been elicited by "Sc" among the three conditions. In
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46
47 addition to some difference currents in left cerebral hemisphere, understanding
48
49
50 unintelligible action in "Sc" condition has evoked extra greater local field potential
51
52
53 activities located at right cortical regions compared to "Ug" and "Tg" conditions (Fig.
54
55
56 5C and 5D). As a part of frontal area known to have mirror neuron properties, the
57
58
59 right IFG with increased activities is more critical for understanding the intentions
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61
62 behind action observation (Lacoboni et al. 2005; Ortigue et al. 2009, 2010). More
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1 importantly, there are concurrently strengthened activities in the mPFC, right STS,
2
3 and anterior temporal pole, which can be closely associated with inferential processes
4
5 of actions, particularly unusual actions (Brass et al. 2007; Ortigue et al. 2009).
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8
9 In previous studies, the ranges of response time of action intention understanding
10
11 are diverse in different experiments, which might be influenced by action type, task
12
13 difficulty, and the context of action execution, *etc* (Van der Cruyssen et al. 2009). The
14
15 identified time interval around 200 ms of microstate 3 is a typical choice of mirror
16
17 response by most studies (Catmur 2015; Cavallo et al. 2014; Naish et al. 2014; Van
18
19 der Cruyssen et al. 2009; Vistoli et al. 2015). Besides, the timing of microstate 5
20
21 (324~700 ms) shows a high overlap with the time interval of intention inference in the
22
23 studies using tasks with the same intention identification difficulty (Ortigue et al.
24
25 2009, 2010), and keeps the consistency with the suggestion that the response latency
26
27 of P3b represents the information processing time or time needed to recognize and
28
29 categorize an unusual event in discriminating oddball and common stimulus (Donchin
30
31 et al. 1978; Johnso and Donchin 1978). Especially in terms of the source distribution
32
33 of ERP difference waves, the spatiotemporal shift from left hemisphere dominance in
34
35 action observation to right hemisphere dominance in intention inference is greatly in
36
37 line with a large amount of neuroimaging studies (Brass et al. 2007; Catmur 2015;
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39 Liew et al. 2011; Ortigue et al. 2009, 2010; Spunt et al. 2011; Van Overwalle and
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41 Baetens 2009).
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55 *Event-related functional connectivity microstates in α frequency band:* The
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57 time-frequency analysis of phase lock among trials shows that the ITC in the α
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1 frequency band remains significant up to 700 ms, *i.e.*, the maximum time of ERP
2
3 response in this task, and the β -band ITC is partly involved in the early time window
4
5 as well (Fig. 2). Over the task course, the functional connectivity of both α - and
6
7 β -band networks adaptively changes with the ERP-indexed neurocognitive functions,
8
9 with more significant between-conditions differences in global topology and local
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11 nodes revealed in α -band functional networks.
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17 Previous studies have suggested that α -band oscillation is related to highly
18
19 specific perceptual, attentional and memory processes, and β -band oscillation is
20
21 mainly associated with motor activity and also plays a role in attentional or other
22
23 higher cognitive function (Sauseng and Klimesch 2008). Moreover, EEG/ERP studies
24
25 have pointed out that α -band phase reset particularly contributes to the generation of
26
27 ERPs, and α phase synchronization is a manifestation of event-related timing
28
29 mechanism of interactive cortical processing (Hanslmayr et al. 2007; Klimesch et al.
30
31 2007). As with the previous suggestions, in this study the ITC in α frequency band
32
33 demonstrates strong phase-locked activities at ERP component latencies, especially
34
35 the N170, P300 and P400 response time. By contrast, β -band ITC is more obvious in
36
37 the earlier period before 200 ms, reflecting the phase-locked oscillations in the β
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39 frequencies strongly related with visual perception of motor activity (Fig. 2).
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50 Due to more exact timing of the cognitive sub-processes indexed by ERPs, the
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52 α -band functional connectivity microstates isolated in the specific temporal windows
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54 probably convey more explicit event-related information of mirroring matching and
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56 intention inference of the action intention understanding task. As a result, the α -band
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1 functional networks exhibit definite hub centrality changes from the AON to the MZN
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3 and reflect the distinguishable features of phase synchronizations between action
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5 intention conditions in this study (Fig. 6-11).
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9 *Adaptive reconfiguration from left-lateral action observation network to*
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11 *bilateral mentalizing network:* Given the timing of the ERP microstates, the analyses
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13 on global topology and local node centrality of functional brain networks have
14
15 discovered two distinctly different structures organized by phase-synchronized
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17 oscillations of N170-P200 and P400-700 responses, salient in the α frequency band.
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19 The topological change indicates the functional switching of the brain from the AON
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21 to the MZN through timely adaptive network reconfiguration.
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28 In "Ug" and "Tg" conditions, the AONs from N170-P200 responses with better
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30 configuration for perceptual information processing than that in "Sc" condition are
31
32 composed of left frontal, premotor-temporal and frontal-parietal-occipital
33
34 communities (Fig. 9), with functionally centralized nodes located at left premotor,
35
36 temporal and inferior parietal cortices (Fig. 8). In the AON structure, the premotor
37
38 cortex plays an important role in identifying the goals or intentions through a direct
39
40 matching process. The anterior IPS is involved in the on-line motor control of
41
42 body-part movements for goal objects (*e.g.*, grasping a cup), and the execution and
43
44 observation of goal-oriented movements. The STS contains polysensory neurons
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46 responding to motion from different perceptual modalities, and outputs information to
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48 the anterior IPS and premotor cortex (Becchio et al. 2012; Catmur 2015; Ortigue et al.
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50 2009; Rizzolatti et al. 2001; Van Overwalle and Baetens 2009; Woodward and Gerson
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1 2014).

2
3 During P400-700 period in "Sc" condition, the MZN structure is more beneficial
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6 for inferential information management. Except for bilateral frontal-parietal and
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8
9 temporal-parietal synchronizations, the MZN formed in "Sc" condition contains
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11 additional involvement of right frontal and frontal-temporal communities. In the MZN
12
13 structure, bilateral fronto-parietal synchronizations underlie fundamental cognitive
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15 control process, and temporal-parietal synchronizations are most crucial for the
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17 representation of goals and intentions in the mentalizing system (Becchio et al. 2012;
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19 Van Overwalle and Baetens 2009). In the additionally involved right frontal area, the
20
21 PFC is critically involved in reflective reasoning about actions and judgments
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23 including goals and intentions (Atique et al. 2011; Ortigue et al. 2009; Van Overwalle
24
25 and Baetens 2009), right IFG is particularly related to intention recognition, and
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27 frontotemporal connectivity facilitates mental activity for executive function and
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29 inference.
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39 ***Complementary effect and causal association between mirror and mentalizing***
40 ***systems:*** The spatiotemporal evolution of the phase-synchronized networks in
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42 understanding different action intentions reflects a functionally complementary effect
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44 between the topological configurations of the AON and the MZN. As compared with
45
46 unintelligible actions, the observation of usual actions ("Ug" and "Tg" conditions)
47
48 induces higher inter-regional connectivity in left premotor-temporoparietal circuit
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50 during the early N170-P200 period when the mirror neuron system is firing, which is
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52 consistent with Gardner et al.'s (2015) finding that movement familiarity dynamically
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1 modulates more activities in cortical areas of AON. In this experimental task, the
2
3 enhanced phase synchronization in the AON is a manifestation of increased
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5 information communication among task-related brain areas when the observed actions
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7 are rather usual in our daily life, *e.g.*, "grasping a cup for drinking" and "grasping a
8
9 cup for moving". By contrast, in "Sc" condition, the mirror function of the brain is
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11 suppressed while the perceived action is outside the observer's repertoire of familiar
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13 movements, presented as lower synchronized activities in the AON. However, in the
14
15 later time window of P400-700 response, the brain areas involved in task-related
16
17 mentalization become more activated, especially the right frontal, temporal and
18
19 parietal cortices where there is increasing involvement of right frontal-temporal and
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21 temporal-parietal synchronizations under "Sc" condition. During this period, the
22
23 increased frontal-temporal connectivity can be associated with strengthened inference
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25 function for detecting intentionality, and the enhanced temporal-parietal interactions
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27 might be responsive for higher effort in estimating the orientation or direction of the
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29 behavior in order to predict its possible end-state (or goal) (Becchio et al. 2012; Brass
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31 et al. 2007; Van Overwalle and Baetens 2009). The variation in dynamic functional
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33 networks supports De Lange et al.'s (2008) finding that part of the mirror-neuron
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35 system is only activated in action perception whereas part of the mentalizing system
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37 becomes active in the recognition of others' intentions, suggesting distinct but
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39 complementary function of the two systems.
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55 The previous studies have been debating whether the mirror and mentalizing
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57 systems are mutually independent or cooperated in human understanding of
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1 intentionality (Becchio et al. 2012; Catmur 2015; Neal and Kilner 2010; Tidoni and
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3 Candidi 2016). Van Overwalle and Baetens (2009) have concluded that neither mirror
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5 nor mentalizing system subserves the other, since the two systems are rarely
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7 concurrently activated. During performing specific tasks, if brain areas subserving one
8
9 system are activated while the areas of the other system are inactive, the two systems
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11 might be well independent. On the other hand, a substantial number of studies support
12
13 the assumption that the two systems work together, and mirror neurons might provide
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15 rapid and intuitive input to the mentalizing system to support and constrain inferential
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17 process (Catmur 2015; Gardner et al. 2015; Tidoni and Candidi 2016; Van Overwalle
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19 and Baetens 2009). In this study, the DFC analysis reveals that the AON and the MZN
20
21 are largely not overlapped in topological structures and show temporally isolated
22
23 enhancement of functional integration among brain areas, which indicates respective
24
25 dominant roles in detecting distinct aspects of human behaviors, *i.e.*, action perception
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27 and intention inference. Although the AON and the MZN have been recruited in
28
29 isolation by this specific task, the DFC under different action intention conditions
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31 indicates that there is implicit causal association between the recruitment of low-level
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33 mirror matching and high-level inference activities. Intention identification of
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35 irrational, implausible or unusual action is cognitively more demanding and
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37 additionally requires observer's mental effort and cognitive load on working out why
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39 it is being performed (Catmur 2015; Van Overwalle 2009; Van Overwalle and Baetens
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41 2009). Previous dynamic network research has demonstrated that mental effort, in
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43 particular, can modulate long-distance functional connectivity among anatomically
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1 separated brain areas (Bassett et al. 2006; Kitzbichler et al. 2011). As a result, when
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3 there is no immediate visual substrate on which to complete intentionality judgments,
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5 effortful cognitive processing for indentifying the intentionality of unintelligible
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7 action would drive greater topological reorganization toward an enhanced MZN
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9 structure with higher global integration and additional involvement of task-related
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11 brain areas, and vise versa. Thus, the acquisition of sensorimotor information from the
12
13 AON can be viewed as a prerequisite of imposing different cognitive workloads on an
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15 observer, which restrain or drive functional integration among cortical area of the
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17 mentalizing system, with working memory serving as the interface between visual
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19 perception and inferential process.
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28 *Potential application of the identified EEG/ERP patterns:* Intention
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30 understanding is a basic requirement for human-machine interaction. Action
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32 classification and brain response recognition are two possible ways to understand
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34 human intention (Yu et al. 2015). The present study reveals the switched functions of
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36 the brain from the AON to the MZN during an action intention understanding task,
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38 with the synchronization differences between task conditions changed from left
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40 frontal-temporal and temporal-parietooccipital to right frontal-temporal-parietal
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42 regions. According to the neurocognitive functions from recognizing action
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44 kinematics to inferring intentionality, feature extraction of phase synchrony was
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46 conducted on EEG electrodes in the temporal windows of N170-P200 and P400-700
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48 responses. The discrimination results from different methods demonstrate that the
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50 time-evolving α -band WPLIs represent identifiable EEG/ERP patterns for
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1 understanding usual action and unintelligible action. Particularly, the best
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3 classification accuracy in the frequency-specific feature combination from the two
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5 temporal windows has been attained at electrode site T7, indicating the adaptiveness
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7 of left temporal lobe in the cooperative interaction with task-related neuronal
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9 populations that are self-organized in understanding usual and unintelligible action
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11 intentions. The EEG sensor-level DFC study provides preliminary evidence for
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13 cognitive detection and intention classification in brain-computer interface (BCI)
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15 applications that require rapid and reliable extraction of discriminatory information
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17 from event-related EEG patterns. According to the justified EEG electrode sites and
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19 cognition-related temporal windows, further single-trial classification for individual's
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21 action intention recognition is worthy to be systematically explored and improved,
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23 such as an effective feature combination from multiple channels with optimized
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25 discriminatory information involved in the switched phase relationship from the AON
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27 to the MZN. Additionally, an action intention understanding paradigm more
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29 appropriate for BCI practice should be considered and developed in the future.
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Figure legends

Fig. 1 Experimental paradigm of "hand-cup interaction" observation task. (A) Three hand-cup interaction actions: a hand grasping a cup for using it (Ug); a hand grasping a cup for moving it (Tg); a hand touching a cup without any obvious purpose (Sc). (B) Timeline of stimulus presentation and time interval of an epoch of EEG data.

Fig. 2 Time-frequency diagrams of inter-trial coherence of principle components at left and right hemispheres. (A) "Ug" (B) "Tg" and (C) "Sc" conditions.

Fig. 3 Grand average of ERPs for the three conditions (*i.e.*, Ug, Tg, and Sc) from channels FZ, CZ, PZ and POZ. Time=0 corresponds to the onset of "hand-cup interaction" presentation. The figures show that each condition has elicited five ERP components that are marked with vertical dotted lines. The blue, green, and red solid lines represent the "Ug", "Tg", and "Sc" conditions respectively.

Fig. 4 Brain microstates and cortical sources activated in the task course, illustrated by EEG data averaged across subjects from the "Ug" condition. Top: EEG in "Ug" condition; Middle: five electric field topologies corresponding to the GFP peaks in EEG duration; Bottom: absolute values of source currents of microstates displayed on MRI viewer and cortical surface.

Fig. 5 Topological maps of GFP and difference waves. Top: brain mapping of (A) N170-P200 microstate and (B) P400-700 microstate in "Ug", "Tg" and "Sc" conditions. Bottom: source current distribution of difference waves on the cortical surface (R: right side; L: left side). The electrodes on the brain maps represent the locations with significant differences in (C) "Sc-Ug", (D) "Sc-Tg", and (E) "Tg-Ug" via the paired t-tests with FDR correction.

Fig. 6 WPLI-based functional microstate networks under the "Ug", "Tg" and "Sc" conditions during continuous temporal windows of ERPs. (A) α and (B) β frequency bands. The functional connections are constructed by setting a fixed threshold for each association matrix. The color marked in an EEG electrode represents "degree" of the node in a network, with the value indicated in the color bar.

Fig. 7 Temporal evolution of global topology of the WPLI-based functional networks under the "Ug", "Tg" and "Sc" conditions. (A) α and (B) β frequency

bands. Top: measures of connection density and characteristic path length in the five microstates; Bottom: statistical results from the paired t-tests between each two conditions for measures of connection density and characteristic path length in the five microstates, with * indicating $p < 0.05$. The blue, green and red curves and bars represent "Ug", "Tg" and "Sc" conditions respectively.

Fig. 8 Topological distributions of node centrality in five functional connectivity microstates: (A) α and (B) β frequency bands. From top to bottom: distribution of nodes with high degree centrality, closeness centrality, and betweenness centrality by selecting the nodes with the highest centrality scores (top 10 from each type of centrality) and further excluding the nodes with too low scores. The electrodes colored in blue, green and red represent the centralized nodes of "Ug", "Tg", and "Sc" conditions respectively.

Fig. 9 Force-directed node layouts and major communities of the functional connectivity microstates in the temporal windows of N170-P200 and P400-700 responses. (A) α and (B) β frequency bands. From top to bottom: "Ug", "Tg" and "Sc" conditions. Each node corresponds to an EEG electrode, and the colors represent different functional communities parsed by the Louvain method.

Fig. 10 WPLI differences between task conditions of the functional connectivity microstates in the temporal of N170-P200 and P400-700 responses. (A) α and (B) β frequency bands. From top to bottom: the networks are constructed by the difference values of WPLIs from "Ug minus Sc", "Tg minus Sc", and "Tg minus Ug". The blue edges indicate increased synchronized node pairs (*i.e.*, positive difference values), and the red edges represent decreased synchronizations (*i.e.*, negative difference values). The width of an edge is proportional to the absolute difference value in comparison. The colored nodes refer to significant difference in connection strength (paired Student's t-tests with a FDR correction: $p < 0.05$), and the color of a node is proportional to its $\log p$ in the paired t-test, with the value indicated in the color bar.

Fig. 11 Feature distributions and discrimination results for node connection strengths in the temporal windows of N170-P200 and P400-700 responses. EEG electrodes (A) T7 at the left temporal lobe, (B) P2 at the right superior parietal lobe and (C) FP2 on the right prefrontal cortex. Top: the scattergram of subject-based samples. The horizontal axis represents the connection strength of an electrode in the temporal window of N170-P200 and the vertical axis P400-700. The blue, green and red markers represent the samples from the "Ug", "Tg", and "Sc" task conditions respectively. Bottom: discrimination accuracy between each two task conditions from

LDA, SVM and Naive Bayes. The outliers in the red circles are excluded from the discriminant analysis according to the fuzz c-means clustering method.

Table 1 Duration and cortical sources of event-related microstates

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Figure 1

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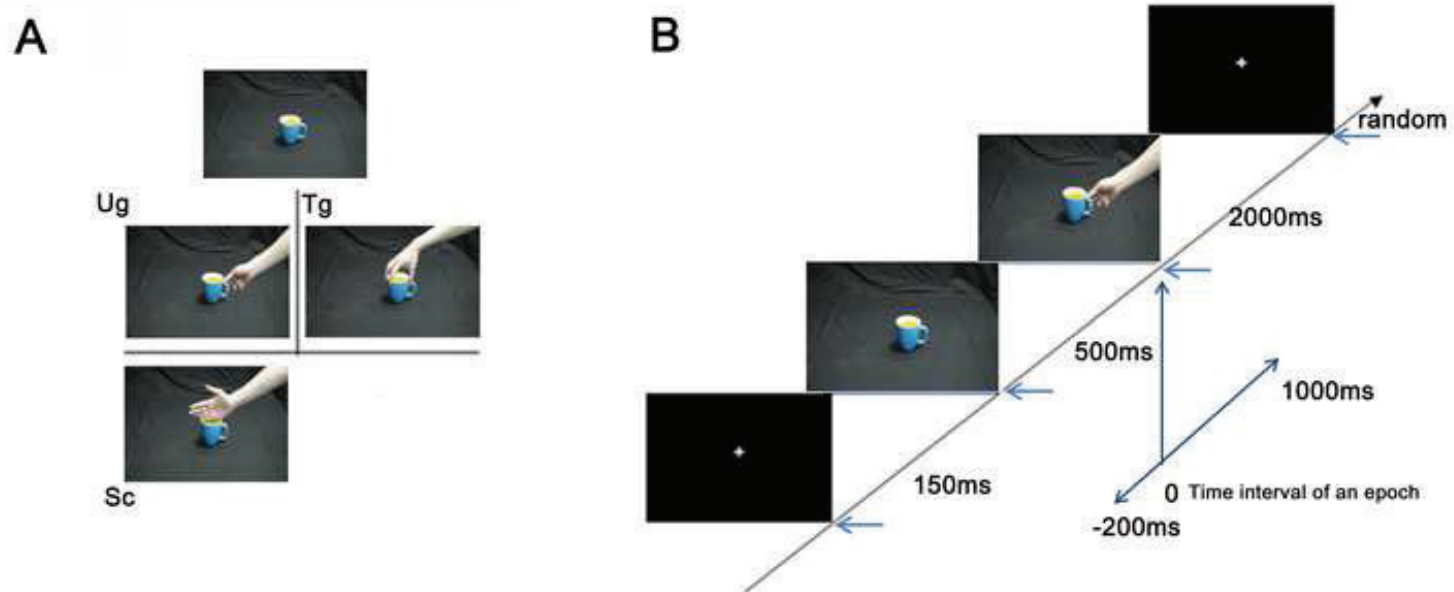


Figure 2

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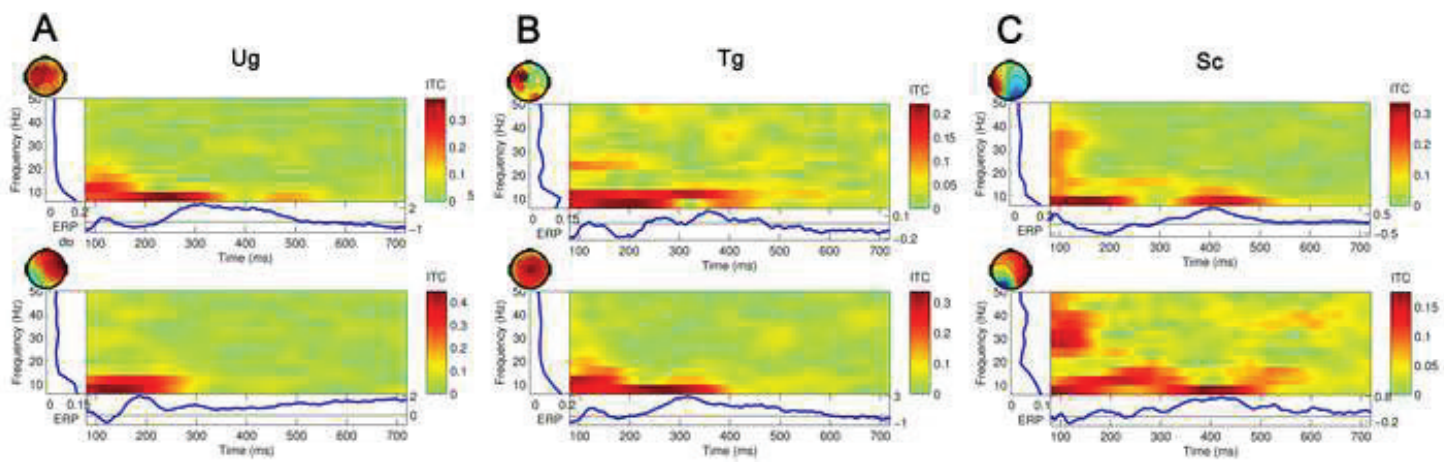


Figure 3

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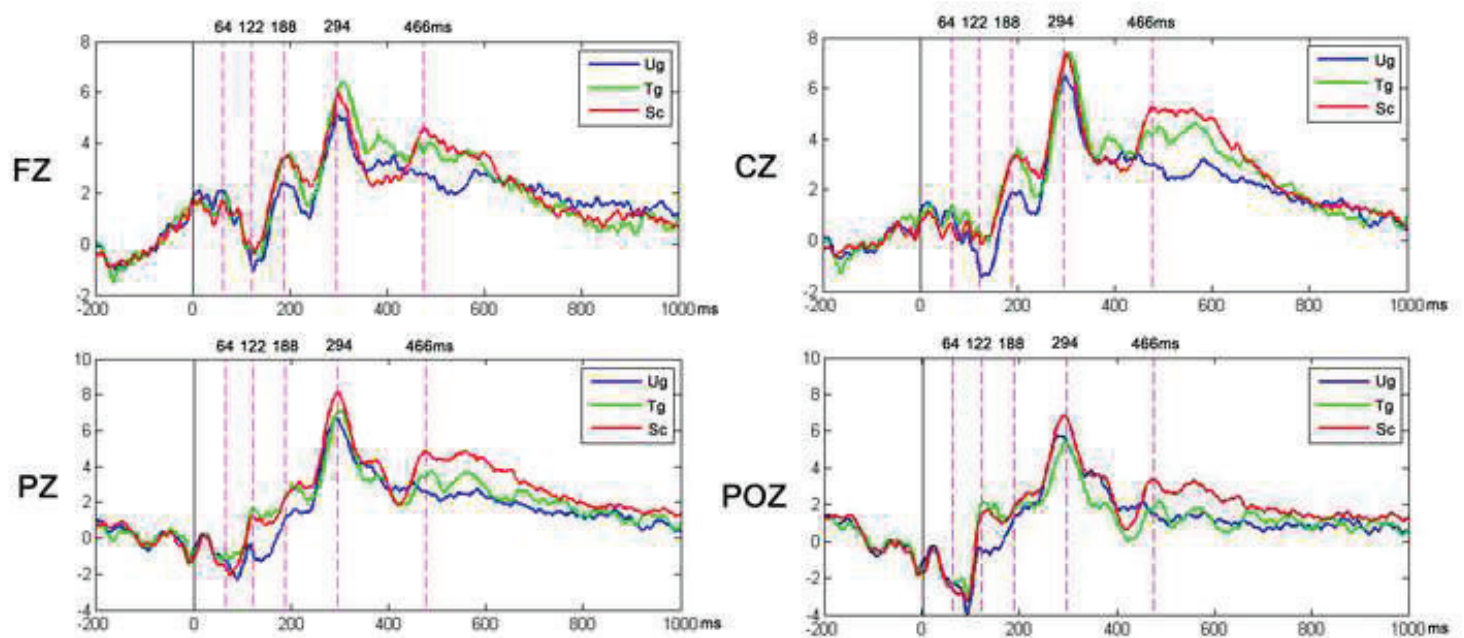
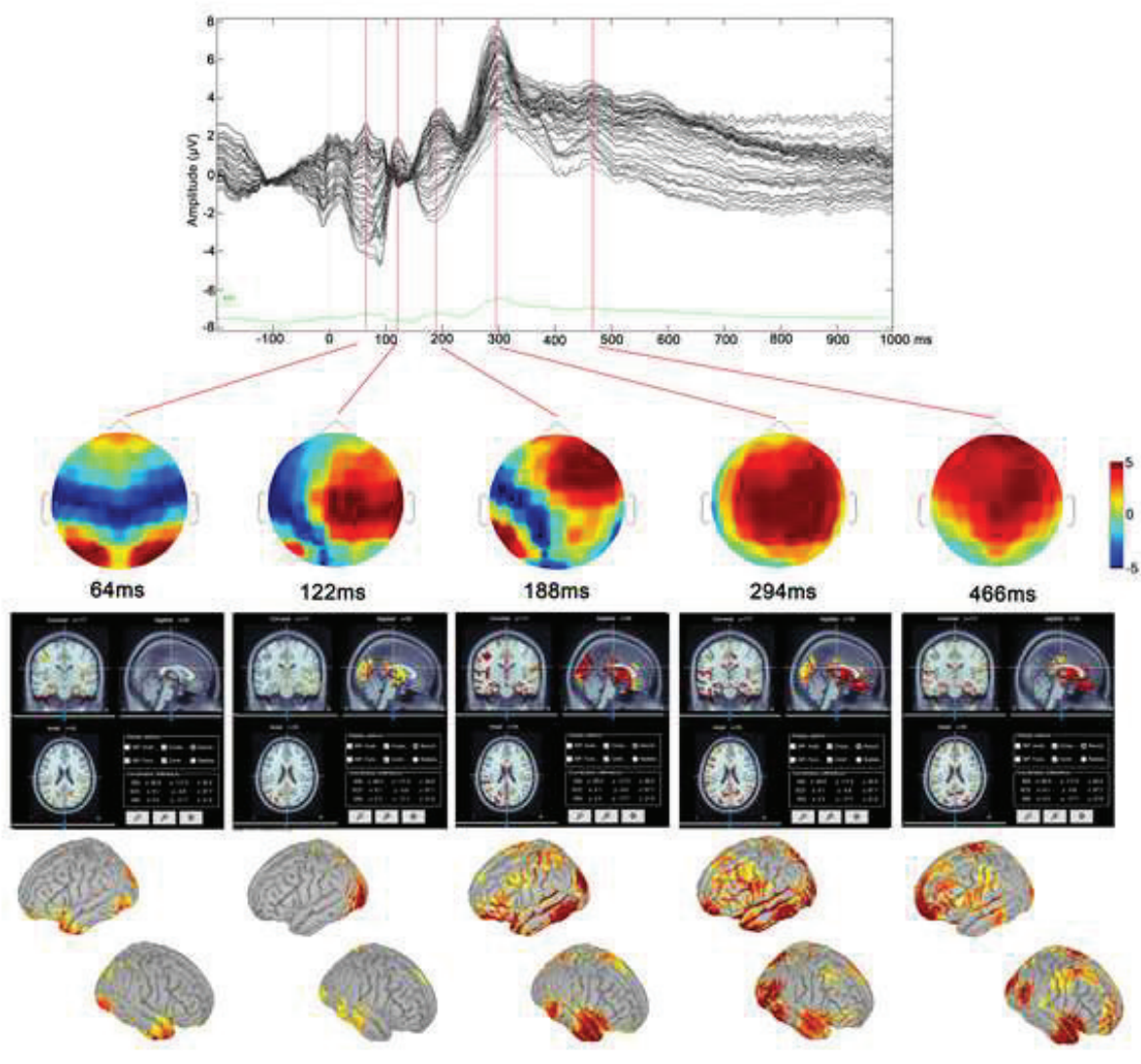
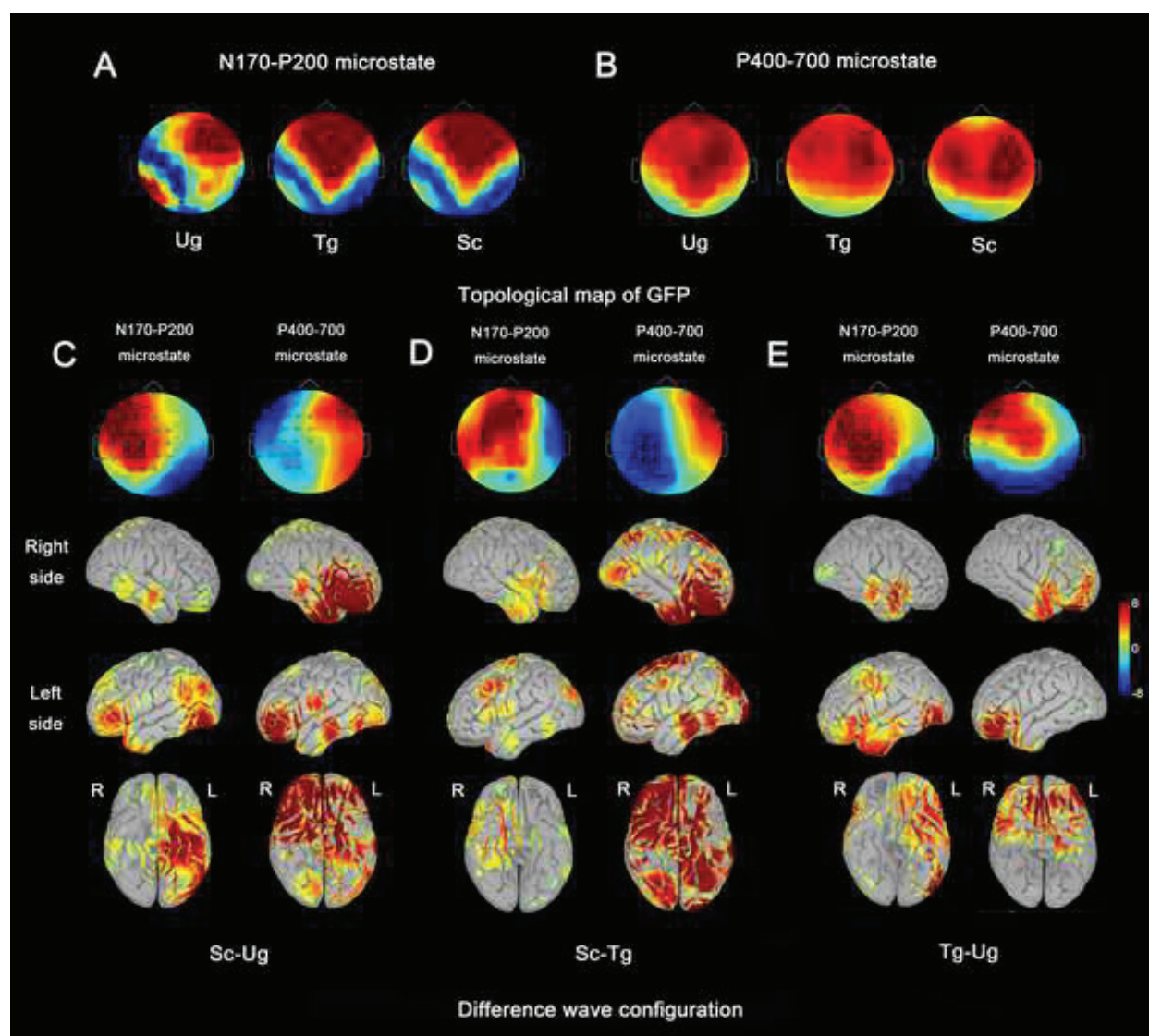
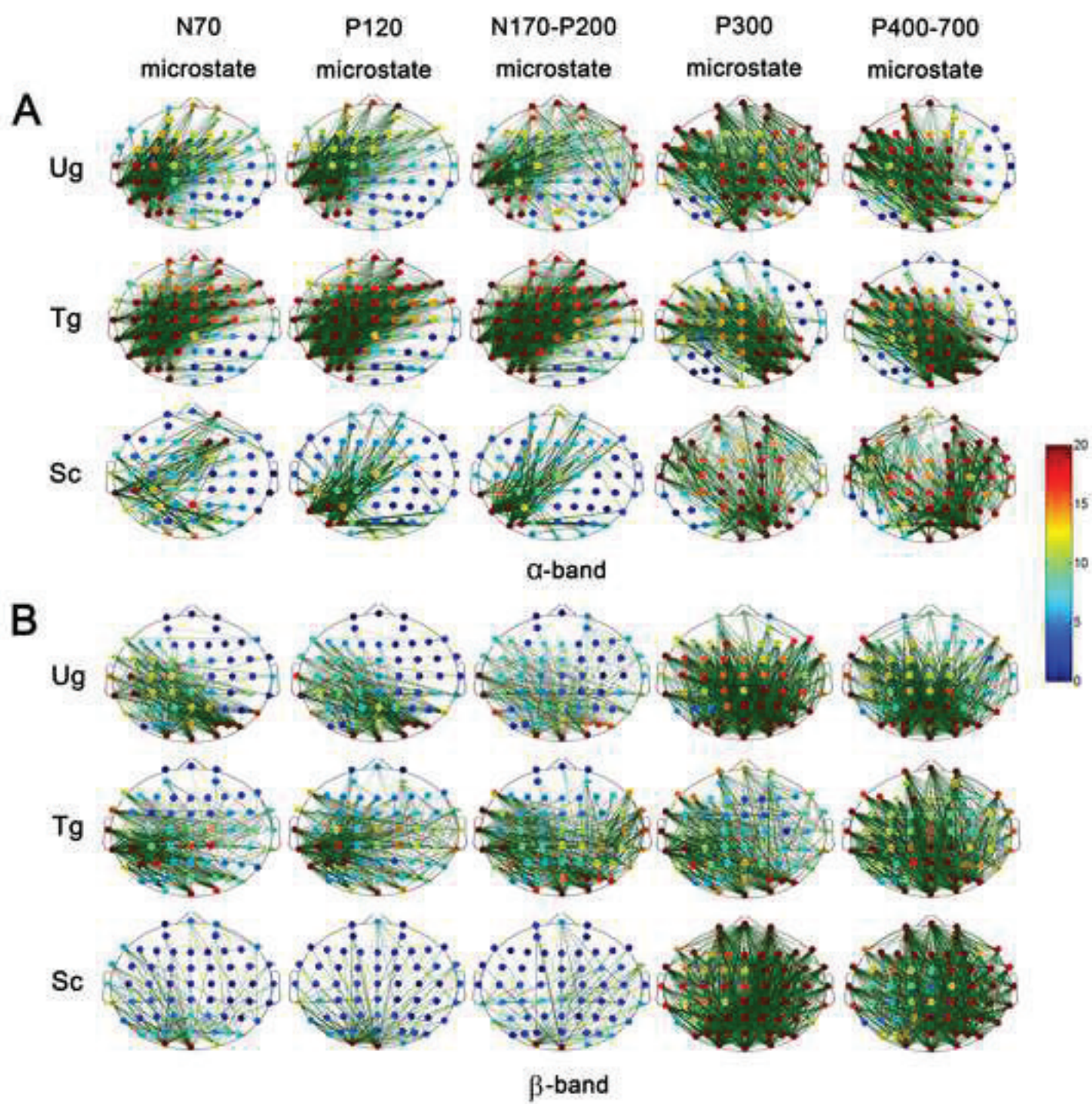


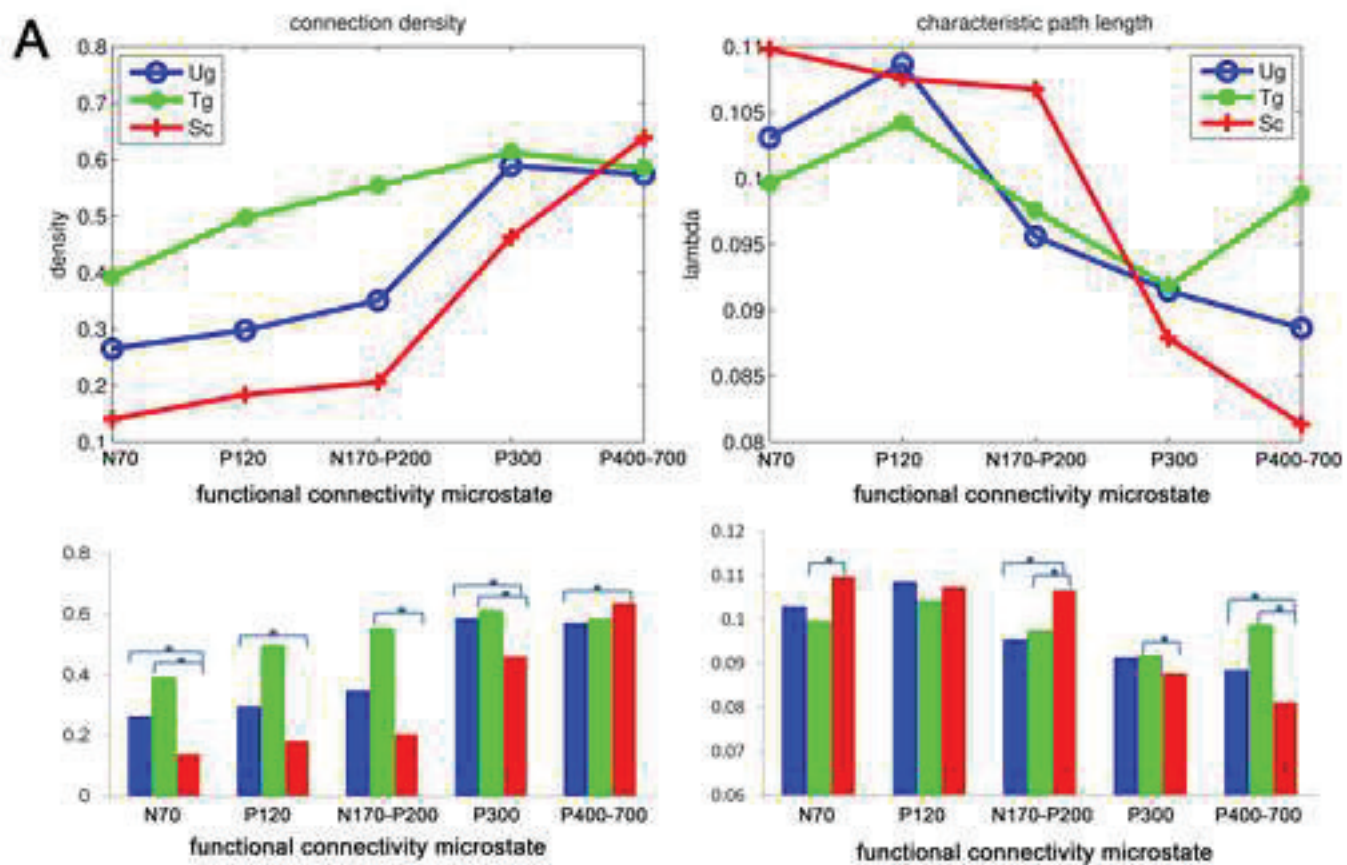
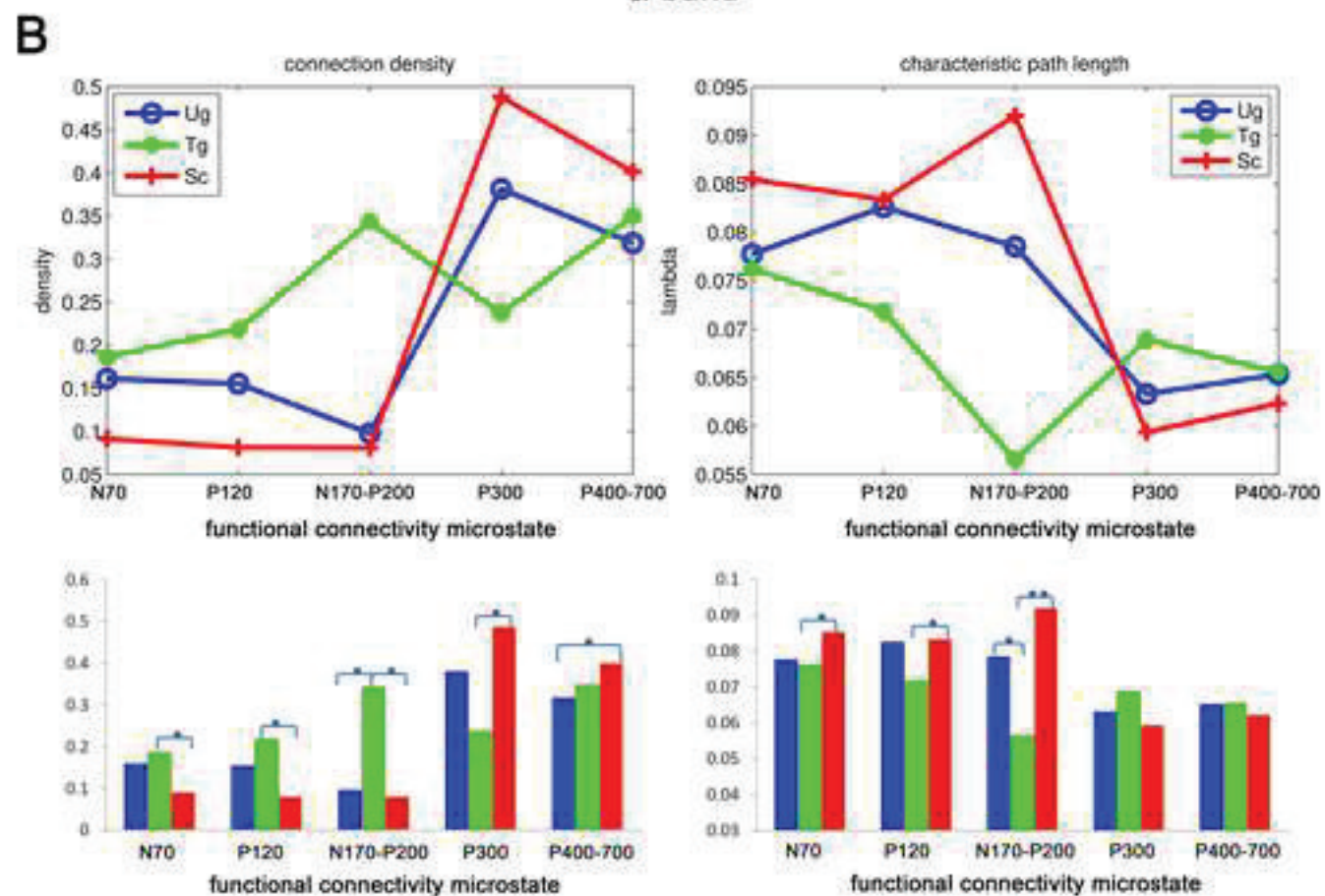
Figure 4

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 α -band β -band

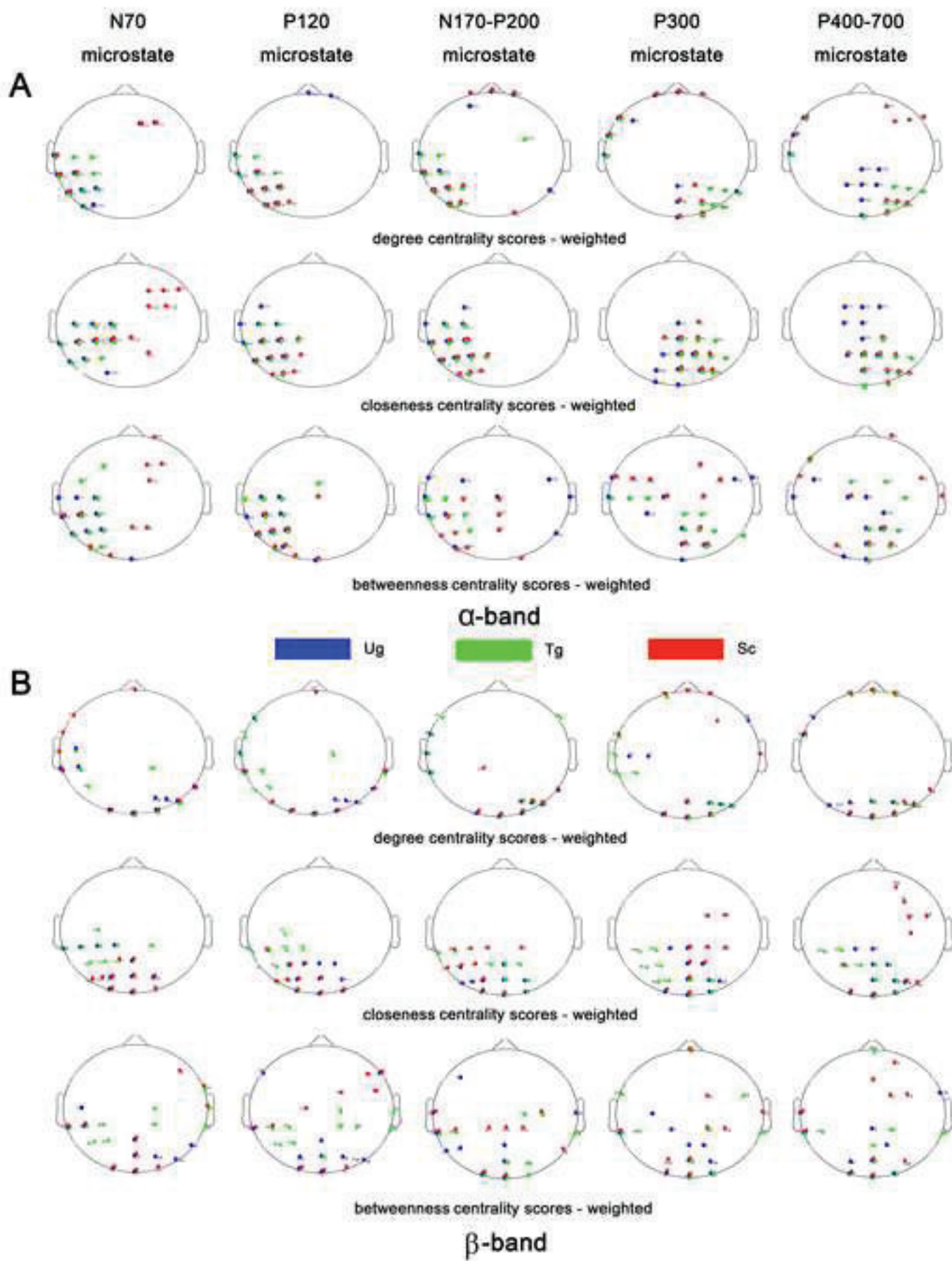


Figure 9

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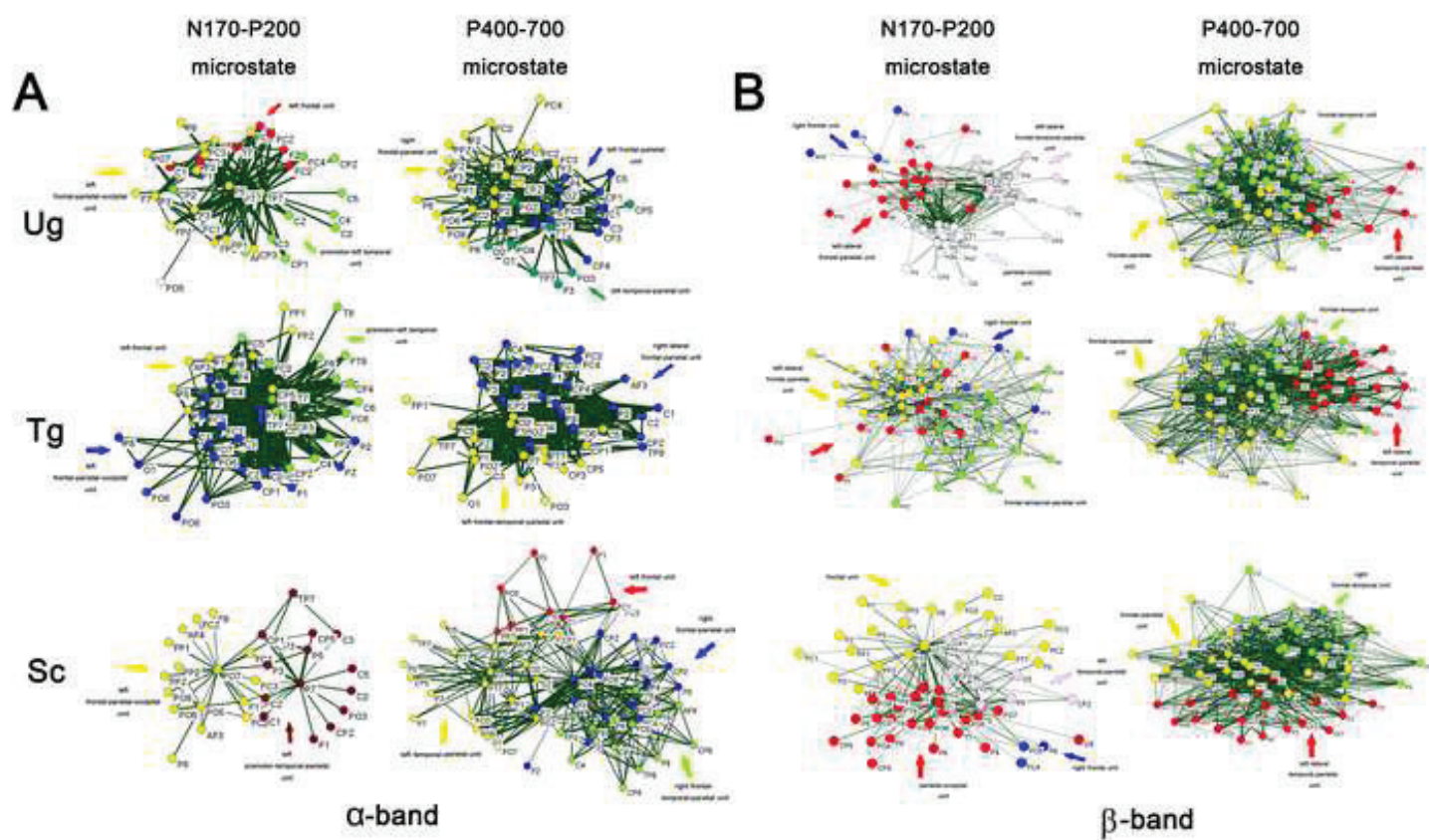


Figure 10

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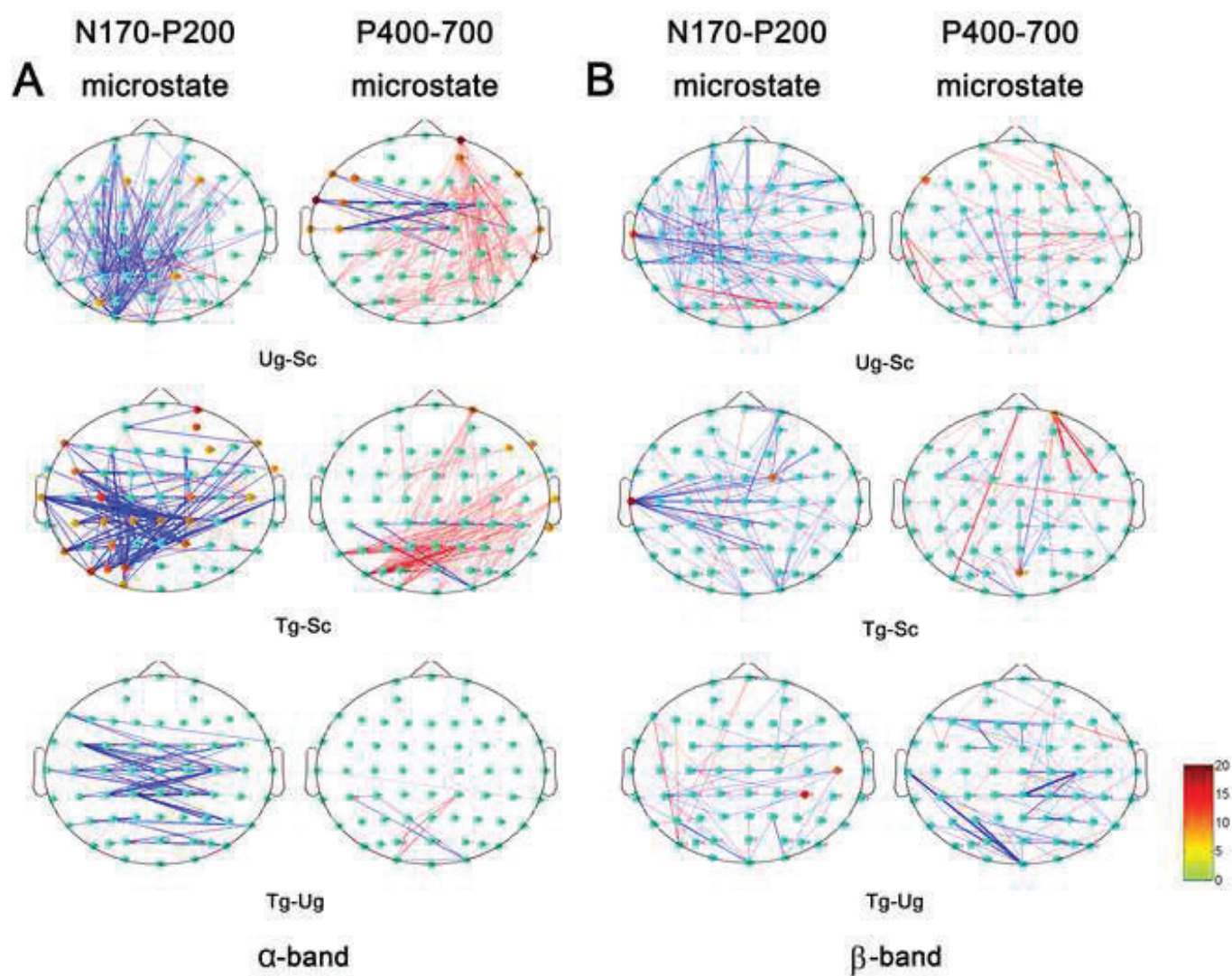


Figure 11

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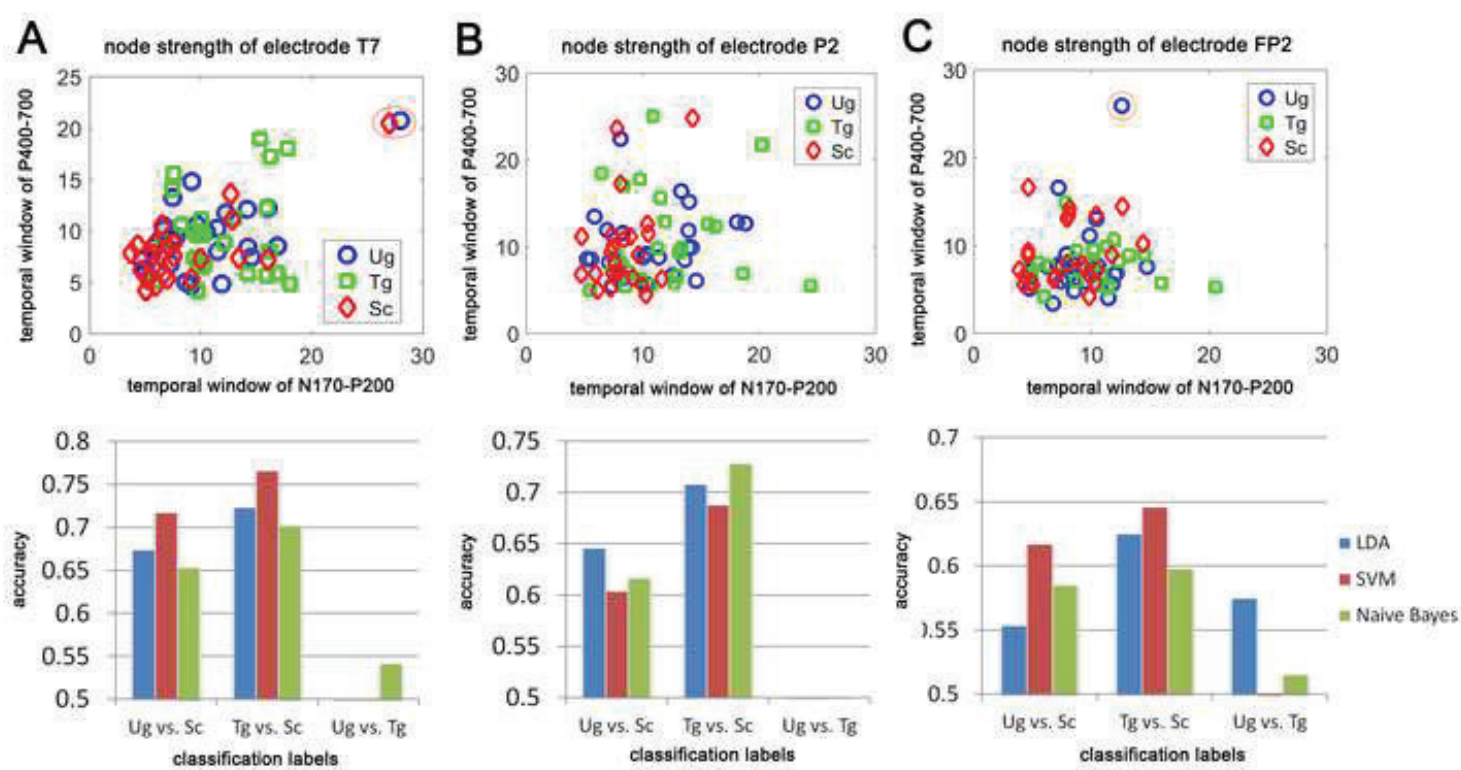


Table 1

Table 1 Duration and cortical sources of event-related microstates

Event-related microstates		microstate 1	microstate 2	microstate 3	microstate 4	microstate 5
ERP component		N70	P120	N170-P200	P300	P400-700
Duration (ms)	Ug	0~94	106-146	164~234	254~312	326~700
	Tg	0~96	106~146	158~258	270~318	330~700
	Sc	0~80	106~150	156~248	274~320	326~700
Cortical sources		occipital cortex	left-lateral parietal and occipital cortices	left-lateral anterior intraparietal sulcus, premotor cortex, superior temporal sulcus, and parietooccipital cortex	anterior cingulate, temporal lobe, parietooccipital cortex and right-lateral temporoparietal cortex	medial prefrontal cortex, anterior cingulate, superior temporal sulcus, right-lateral anterior temporal pole and temporoparietal cortex